## THE LANCET Neurology

## Supplementary webappendix

This webappendix formed part of the original submission and has been peer reviewed. We post it as supplied by the authors.

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## WEB EXTRA MATERIAL

## Supplementary methods:

## Disease overview

Inclusion body myositis (IBM) is an acquired inflammatory myopathy with onset usually over 50 years of age with a male predominance and the quadriceps being the predominant muscle affected in the lower limbs. There are currently no treatments with proven efficacy despite numerous trials. ${ }^{1}$ Charcot-Marie-Tooth disease (CMT) is an umbrella term for the hereditary motor and sensory neuropathies with a combined prevalence of around 1:2500 and over 70 causative genes identified. The most common type is CMT1A representing $50 \%$ of all CMT with progressive distal weakness from childhood. ${ }^{2}$ Recent trials have been hampered by insensitive outcome measures. ${ }^{3}$

## Exclusion criteria: (all subjects)

- Concomitant neuropathy/myopathy
- Very advanced disease state that precludes travelling
- Severe cardiovascular, renal, or other end-stage-organ-disease states or any other major comorbidities (e.g. any active malignancy, definite cognitive impairment, psychiatric disease, heart or lung failure, orthopedic or rheumatologic disorders)
- Pregnancy and active nursing (breast feeding)
- Inadequate contraception in women of child bearing age.
- Contra-indication to MRI (metallic fragments, clips or devices in the brain, eye, spinal canal, etc; magnetically activated implanted devices, such as cardiac pacemakers, insulin pumps, neurostimulators and cochlear implants; claustrophobia)
- Existing radiculopathy or lower back pain
- Surgery to feet within 12 months of beginning of study or during the study


## Clinical Strength Grading (MRC Scale)

The following movements were assessed:

- Neck: flexion and extension
- Upper limbs: shoulder abduction, elbow extension, elbow flexion, wrist extension, wrist flexion, finger extension, forefinger abduction, little finger abduction, thumb abduction, long finger flexors, short finger flexors
- Lower limbs: hip flexion, hip extension, hip abduction, hip adduction, knee flexion, knee extension, ankle dorsiflexion, ankle plantarflexion, ankle eversion, ankle inversion, big toe extension
Muscle strength was assessed using a modified MRC scale ${ }^{5}$ with 5: normal strength, 5-: barely detectable weakness, 4+: gravity and moderate to maximal resistance, 4: Gravity and moderate resistance, 4-: Gravity and minimal resistance, 3: Full range of motion against gravity only, 2: Movement when gravity is eliminated, 1: Flicker of movement seen or felt, 0 : No movement. Upper limb/neck and lower muscle scores were summed to obtain a total upper limb/neck and total lower limb score for each subject. For this purpose 5- was scored as $4.75,4+$ as 4.25 and 4 - as 3.75 . The maximum score obtainable was 120 upper limb/neck and 110 for lower limb.


## Myometry protocol

All but two initial assessments and all follow up assessments were performed by a single neurologist. Myometry was performed according to the table below. Knee extension, knee flexion, ankle dorsiflexion, and ankle plantarflexion were assessed bilaterally using both isometric and isokinetic protocols and the maximum torque in Nm recorded for analysis. Isometric assessments consisted of four attempts of 3 seconds duration with 10s interval of which the best attempt was selected. For the isokinetic assessments, following a practice run and 10 s interval, three successive movements through full range were performed and the highest value obtained selected. The machine setup was recording at first visit using the included software, which was then retrieved to allow identical set-up on repeat testing. A single observer performed over $90 \%$ of assessments. All measurements are stored within the HUMAC NORM system, and were checked for artefacts before being exported into IBM-SPSS for analsysis. An additional overall strength for each movement was calculated by taking the mean of all assessment methods. The Myometry assessment either occurred following the MRI or with at least a 60 minute gap if preceding to minimise any potential MRI effects secondary to physical activity.

| Joint | Type | Movement | Angle |
| :---: | :---: | :---: | :---: |
| Knee (right then left) | Isometric | Extension ${ }^{\circ}$ | $45^{\circ}$ |
|  |  | Extension | $90^{\circ}$ |
|  |  | Flexion | $45^{\circ}$ |
|  |  | Flexion | $90^{\circ}$ |
|  | Isokinetic | Extension/Flexion | $60^{\circ} \mathrm{s}$ |
|  |  | Extension/Flexion | $120 \%$ s |
| Ankle (left then right) | Isometric | Plantarflexion | $10^{\circ}$ |
|  |  | Dorsiflexion | $10^{\circ}$ |
|  | Isokinetic | Plantarflexion/Dorsiflexion | $60^{\circ} \mathrm{s}$ |

## MRI Protocol

## Selection of musculature

Lower limb muscles were chosen as the region for study as they are a key site of pathology in both CMT1A (lower calf) $)^{2}$ and IBM (quadriceps) ${ }^{1}$ and weakness is these areas is a key cause of disability in these patient groups. Furthermore lower limb imaging is practical compared with dedicated upper limb image: both limbs may be imaged simultaneously lowering scanning times and lower limb imaging is in our experience more comfortable for participants.

## Block positioning

Imaging was performed using a multi-channel peripheral angiography coil (Siemens 'PA Matrix') and 'spine matrix' coil elements supplemented with a body surface coil for proximal thighs. Before scanning the distance between the anterior superior iliac spine and the superior border of the patella was measured and thigh-level imaging volumes were centred one third of this distance above the patella superior border. Similarly calf-level imaging volumes were centred below the tibial tuberosity by one quarter of the total distance from the tibial tuberosity to the lateral malleolus. The derived distances were recorded and used for follow up imaging.

## Field of View (FOV)

Both limbs were scanned within the FOV. Axial FOVs were $41 \times 20.5 \mathrm{~cm}$ (thigh) and $40 \times 18.8 \mathrm{~cm}$ (calf)

## 3-Point Dixon Fat-Fraction (FF) Quantification

For Dixon FF measurements, ${ }^{6}$ three 2D gradient-echo acquisitions were performed with echo-times
(TE1/TE2/TE3 $=3.45 / 4.60 / 5.75 \mathrm{~ms}$, TR $=100 \mathrm{~ms}$, flip angle $=10^{\circ}$, bandwidth $420 \mathrm{~Hz} /$ pixel, $\mathrm{NEX}=4,10 \times 10 \mathrm{~mm}$ slices with 10 mm gap, $512 \times 256$ matrix (thigh), $512 \times 240$ matrix calf, iPat=2). Phase unwrapping was performed using PRELUDE (FSL, FMRIB, Oxford $)^{7}$ and after fat ( F ) and water (W) image decomposition, FF calculated as $\mathrm{FF}=100 \% \times \mathrm{F} /(\mathrm{F}+\mathrm{W})$.

The $\mathrm{TE}=3.45 \mathrm{~ms}$ image was used for the region of interest (ROI) placement and as a reference for inter-method image interpolation and registration (calf) using FLIRT (FSL, FMRIB, Oxford), such that that the same ROIs could be applied to extract data from all maps.

## T2-Relaxometry

Dual-contrast turbo-spin-echo (TSE) images ( $6500 / 13 / 52 \mathrm{~ms}$ or $6500 / 16 / 56 \mathrm{~ms}$; 10 x 10 mm slices with 10 mm gap, iPat=2, $\mathrm{BW}=444 \mathrm{Hx}$ /pixel, refocusing flip angle $180^{\circ}$, NEX $=1,6 / 8 k$-space sampling, $256 \times 128$ matirx (thigh), $256 \times 120$ matrix (calf)) were acquired. Pseudo- $T_{2}$ was calculated from the respective pixel intensities $I_{T E 1}$ and $I_{T E 2}$ from the $T_{1}$ and $T_{2}$ images as $T_{2}=$ $\frac{T E_{2}-T E_{1}}{\ln \left(I_{T E 1} / I_{T E 2}\right)}$. The different echo times were the result of altered constraints following a routine scanner software upgrade which occurred after 54 baseline and 6 follow-up scans had been completed. Analysing control values pre- and post-upgrade suggested a systematic bias between pre- and post-upgrade T2 values. By comparing the observed relationship between FF and T2 measurements pre- and post-software upgrade a correction equation was determined separately for thigh muscles (corrected $\mathrm{T} 2=$ 1.0606 x post-upgrade $\mathrm{T} 2+1.1522$ ) and calf muscles (corrected $\mathrm{T} 2=1.0933 \times$ post-upgrade $\mathrm{T} 2-0.0245$ ). These corrections were applied to all post-upgrade T2 measurements to ensure pre- and post-upgrade T2 measurements were comparable. Parameters for the other quantitative sequences were not affected by this upgrade, and analysis of the control values pre- and post-upgrade indicated no systematic bias in these values was introduced by the software upgrade.

## $\mathrm{B}_{1}$ Mapping

Separate TSE images (TR/TE=7000/11ms, 128x64 matrix, 40 contiguous 10 mm slices, $B W=429 \mathrm{Hx} /$ pixel, $1 / 2 k$-space sampling) yielded image intensities $V_{1}$ and $V_{2}$ acquired with nominal excitation $\alpha_{1}$ and $\alpha_{2}$ of $60^{\circ}$ and $120^{\circ} . B_{1}$ deviation was mapped
according to $B_{1 \text { Dev }}=\arccos \left(V_{2} / 2 V_{1}\right) / \alpha_{1}{ }^{8}$

## Magnetization Transfer Ratio (MTR) Imaging

MTRs were calculated from two 3D-FLASH images with $\left(\mathrm{M}_{1}\right)$ and without $\left(\mathrm{M}_{0}\right)$ an MT pre-pulse $\left(500^{\circ}\right.$ amplitude, 1200 Hz offset, 10 ms duration ) $\left(\mathrm{TR} / \mathrm{TE}=65 / 3 \mathrm{~ms}\right.$ or $68 / 3 \mathrm{~ms}, \alpha=10^{\circ}, \mathrm{BW}=440 \mathrm{~Hz} /$ pixel, $\mathrm{NEX}=1,6 / 8 \mathrm{k}$-space sampling, $\mathrm{iPat}^{2}=2,40 \times 5 \mathrm{~mm}$ longitudinal phase encoding partitions, $256 \times 128$ matrix (thigh), $256 \times 120$ matrix (calf)) according to MTR $=\left(\mathrm{M}_{0}-\mathrm{M}_{1}\right) / \mathrm{M}_{0} \times 100$ percentage units (p.u.). Percentage units were used by convention to avoid ambiguity with fractional change expressed as a percentage. ${ }^{9}$ MTR maps were RF-inhomogeneity corrected using the $B_{1}$ maps according using a mean-over-all-subjects $B_{1}$ inhomogeneity correction factor of $k=0.0085 .^{10}$

## Analysis Slice Selection

For the baseline scan the fifth most superior slice was used in the thigh and the sixth slice in the calf unless all muscles were not visible in which case an adjacent slice was selected. The ROI were drawn on the follow up acquisition on the slice closest to that used for the first scan, determined on the basis of measured distance from bony landmarks (tibial plateau or tip of the fibular head) identified on the 3D-FLASH images.
After extraction, all data were cross-checked for outliers and any errors rectified.

## Data analysis

Whole muscle ROIs were defined to encompass the entire muscle cross sectional area (CSA) to the fascia whilst "small" ROIs were defined in a consistent anatomical location within each muscle to avoid contamination with fascia or vessels and to allow for minor anatomical movement between acquisitions (figure 2A). Left and right limb ROIs were defined for all muscles at these levels: rectus femoris, vastus lateralis, vastus intermedius, vastus medialis, semimembranosus, semitendinosus, biceps femoris, adductor magnus, sartorius, gracilis, tibialis anterior, peroneus longus, lateral gastrocnemius, medial gastrocnemius, soleus and tibialis posterior muscles.

Minor adjustments to small ROI were made where imperfect registration meant ROI were no longer wholly within the target muscle. Whole muscle ROIs were transferred to the inherently co-registered FF maps only. The whole muscle ROIs from the unprocessed Dixon acquisition were not used for T2 and MTR analysis to avoid ROI contamination with non-muscle tissue, a particular problem for these measures, at the region boundaries due to minor subject movement between acquisitions. ROIs including areas of gross artefact were excluded from the analysis. Of 248 total maps, 5 fat fraction maps (2\%), 2 T2 maps (1\%) and 14 MTR maps ( $5 \%$ ) were excluded due to technical issues or widespread artefact. Artefact in the anterior right thigh of the MTR maps limited analysis in this region as reported in the application of this protocol to healthy volunteers. ${ }^{4}$ This is demonstrated in the number of each ROI analysed in figure e1.

## Statistical methods

If the follow-up duration differed from 12 months the magnitude of change was converted to an annualised value. Outcome measure 12 month SRMs were calculated for each measure as the mean change between baseline and follow-up divided by the standard deviation of that change, and categorised by magnitude according to Cohen's suggestion: $<0 \cdot 2$ minimal responsiveness; $0 \cdot 2-0 \cdot 5$ small responsiveness; $0 \cdot 5-0 \cdot 8$ moderate responsiveness; $>0 \cdot 8$ large responsiveness.

Table e1: Baseline myometry statistics by group

| Movement | Type | Side/angle | CMT | Control (CMT) | IBM | Control (IBM |
| :---: | :---: | :---: | :---: | :---: | :---: | :---: |
| Knee Extension | Isometric | Right at $45^{\circ}$ | $111.1 \pm 48.9$ (24-209) | $155.6 \pm 47.3$ (73-259) | $35.4 \pm 38.4$ (0-146) | $138.6 \pm 60$ (18-259) |
|  |  | Left at $45^{\circ}$ | $109.7 \pm 47.6$ (38-217) | $152.2 \pm 45.5$ (73-231) | $33.5 \pm 38.3$ (0-145) | $138.9 \pm 48.7$ (62-218) |
|  |  | Right at $90^{\circ}$ | $112.2 \pm 58.4$ (45-290) | $159.3 \pm 62.6$ (84-292) | $29.2 \pm 23.9(2-91)$ | $136.6 \pm 55.4(18-252)$ |
|  |  | Left at $90^{\circ}$ | $106.6 \pm 60.8$ (43-277) | $142 \pm 50.5$ (72-247) | $28.3 \pm 26.5$ (0-94) | $128.5 \pm 43.3$ (72-216) |
|  | Isokinetic | Right at $60 \%$ s | $87 \pm 45$ (12-184) | $133.5 \pm 49.1$ (49-239) | $25 \pm 22(0-87)$ | $116.8 \pm 45.4$ (18-190) |
|  |  | Left at $60 \%$ s | $87.4 \pm 42.1(23-165)$ | $127.6 \pm 40$ (52-202) | $24.2 \pm 24.4(0-94)$ | $115.7 \pm 38$ (52-174) |
|  |  | Right at $120 \%$ s | $70 \pm 32.5$ (27-138) | $106.9 \pm 40.8$ (41-206) | $20.2 \pm 18.3$ (0-71) | $93 \pm 38.5$ (13-170) |
|  |  | Left at $120^{\circ} / \mathrm{s}$ | $68.6 \pm 35.3$ (26-138) | $102.5 \pm 35.2(45-165)$ | $19 \pm 19.7(0-80)$ | $91.4 \pm 32.8$ (45-145) |
| Knee <br> Flexion | Isometric | Right at $45^{\circ}$ | $65.8 \pm 26.9$ (33-115) | $86.6 \pm 28.9(53-141)$ | $49.6 \pm 27.4(2-110)$ | $80 \pm 29.1$ (33-140) |
|  |  | Left at $45^{\circ}$ | $66.3 \pm 27.5(33-113)$ | $81.8 \pm 22.9$ (35-132) | $48.8 \pm 25.5$ (2-106) | $74.9 \pm 27.7$ (35-132) |
|  |  | Right at $90^{\circ}$ | $47.9 \pm 20.4$ (14-92) | $64.7 \pm 27.1$ (31-127) | $28.9 \pm 18.1$ (0-68) | $54.7 \pm 18.9$ (26-106) |
|  |  | Left at $90^{\circ}$ | $45.4 \pm 20.9$ (15-83) | $57.8 \pm 24.3(28-110)$ | $31.3 \pm 20.9(0-77)$ | $49.3 \pm 18.3$ (24-95) |
|  | Isokinetic | Right at $60^{\circ} / \mathrm{s}$ | $46.6 \pm 18.8$ (9-81) | $70 \pm 21.7(28-123)$ | $34.9 \pm 21.4$ (0-81) | $64.5 \pm 21$ (27-99) |
|  |  | Left at $60 \%$ s | $45.1 \pm 20(8-85)$ | $62.9 \pm 17.3$ (20-85) | $37 \pm 21.5(0-80)$ | $62.4 \pm 22.7$ (20-104) |
|  |  | Right at $120 \%$ s | $35.1 \pm 16.8$ (14-72) | $55.5 \pm 19.7$ (22-102) | $26.1 \pm 17.7(0-72)$ | $50.8 \pm 17.8(22-87)$ |
|  |  | Left at $120 \%$ s | $34.5 \pm 18.6$ (12-75) | $50 \pm 14.9$ (20-77) | $25.9 \pm 17(0-57)$ | $48.5 \pm 18.2$ (20-84) |
| Ankle Plantarflexion | Isometric | Right at $10^{\circ}$ | $33.7 \pm 19.6$ (1-64) | $66.6 \pm 20.8$ (35-106) | $34.4 \pm 18.7$ (3-64) | $56.2 \pm 19.1$ (28-92) |
|  |  | Left at $10^{\circ}$ | $32.7 \pm 19.8(0-64)$ | $65.1 \pm 19.5$ (33-108) | $33.6 \pm 16.7(4-60)$ | $57.2 \pm 23.7$ (33-110) |
|  | Isokinetic | Right at $60 \%$ s | $18.7 \pm 12.8(5-58)$ | $57.7 \pm 21.6$ (24-107) | $24.1 \pm 14.3$ (0-54) | $46.1 \pm 17$ (22-75) |
|  |  | Left at $60 \%$ s | $19 \pm 12.4$ (4-53) | $58.6 \pm 21.7(22-115)$ | $29.2 \pm 17.2(7-71)$ | $46.9 \pm 20.5$ (8-79) |
| Ankle Dorsiflexion | Isometric | Right at $10^{\circ}$ | $9.7 \pm 8.1(0-31)$ | $35.7 \pm 13.7$ (16-60) | $15 \pm 12.9(0-38)$ | $33 \pm 14.9$ (7-60) |
|  |  | Left at $10^{\circ}$ | $10 \pm 7.8(0-27)$ | $34.5 \pm 13.1$ (12-58) | $15.4 \pm 12.5(0-38)$ | $32.6 \pm 14.2(8-58)$ |
|  | Isokinetic | Right at $60 \%$ s | $11.9 \pm 8.4$ (0-30) | $25.4 \pm 8.5$ (12-42) | $11.8 \pm 12.5$ (0-50) | $23.3 \pm 9.2$ (9-42) |
|  |  | Left at $60 \%$ s | $11.9 \pm 11(0-43)$ | $24.5 \pm 8.7$ (7-37) | $11.8 \pm 8.3$ (0-26) | $23.2 \pm 9(7-35)$ |
| Ankle Inversion | Isometric | Right at $0^{\circ}$ | $15.6 \pm 10(0-37)$ | $20.4 \pm 7.1$ (9-33) | $11.9 \pm 7.3$ (0-27) | $18.1 \pm 6.4$ (9-33) |
|  |  | Left at $0^{\circ}$ | $14.8 \pm 10.4(0-45)$ | $20.1 \pm 7.1$ (7-30) | $11.5 \pm 6.7$ (0.15-26) | $17.7 \pm 6.7(7-30)$ |
|  | Isokinetic | Right at $60 \%$ s | $16 \pm 9.9(0-38)$ | $25.4 \pm 7.9$ (11-39) | $14.9 \pm 9.6$ (3-34) | $22.7 \pm 7.8$ (9-34) |
|  |  | Left at $60 \%$ s | $14.3 \pm 9.5$ (3-35) | $25.6 \pm 8.9$ (11-43) | $17.1 \pm 10.2(3-35)$ | $21.8 \pm 8.6$ (11-39) |
| Ankle Eversion | Isometric | Right at $0^{\circ}$ | $7.1 \pm 4.1(1-14)$ | $22 \pm 7.6$ (9-37) | $9.6 \pm 5.9(0-22)$ | $19 \pm 7.6(9-34)$ |
|  |  | Left at $0^{\circ}$ | $7.7 \pm 4.8(0-18)$ | $21.4 \pm 7.1$ (11-34) | $10.2 \pm 6.5(0-20)$ | $17.5 \pm 6.9$ (8-31) |
|  | Isokinetic | Right at $60 \%$ s | $8.4 \pm 4(1-15)$ | $17.3 \pm 5.6$ (9-28) | $9.2 \pm 5(0-20)$ | $15.1 \pm 5.6$ (8-23) |
|  |  | Left at $60 \%$ s | $7.8 \pm 3.1$ (3-14) | $17.4 \pm 5.8$ (9-30) | $9.3 \pm 5.8(0-24)$ | $16.2 \pm 7.1$ (8-33) |

Data are mean $\pm$ standard deviation (range). Isometric values are the peak torque at the fixed angle listed whilst isokinetic values are the peak torque at the fixed speed noted. Both CMT1A patients and IBM patients have significantly ( $\mathrm{p}<0.01$ for all) reduced strength than their matched control groups for all measurements.


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Table e4: Linear regression of quantitative MRI variables at baseline, at thigh and calf level with all groups combined

|  | Thigh |  | Dependant variable |  |  |
| :---: | :---: | :---: | :---: | :---: | :---: |
|  |  |  | FF | T2 | MTR |
|  | FF | R |  | 0.92 | 0.93 |
|  |  | Constant |  | 42.6 | 31.8 |
|  |  | Slope |  | 1.35 | -0.38 |
|  | T2 | R | 0.92 |  | 0.95 |
|  |  | Constant | -26 |  | 42.2 |
|  |  | Slope | 0.63 |  | -0.25 |
|  | MTR | R | 0.93 | 0.95 |  |
|  |  | Constant | 73 | 155 |  |
|  |  | Slope | -2.27 | -3.55 |  |


|  | Calf |  | Dependant variable |  |  |
| :---: | :---: | :---: | :---: | :---: | :---: |
|  |  |  | FF | T2 | MTR |
|  | FF | R |  | 0.93 | 0.96 |
|  |  | Constant |  | 41.6 | 31.7 |
|  |  | Slope |  | 1.19 | -0.35 |
|  | T2 | R | 0.93 |  | 0.97 |
|  |  | Constant | -29 |  | 43.2 |
|  |  | Slope | 0.73 |  | -0.28 |
|  | MTR | R | 0.96 | 0.97 |  |
|  |  | Constant | 84 | 149 |  |
|  |  | Slope | -2.61 | -3.38 |  |

Linear regression of pair-wise comparison of quantitative MRI parameters on an individual muscle basis at thigh and calf level. For example at thigh level the equation $\mathrm{T} 2=42.6+0.92 \mathrm{x}$ fat fraction fits data best, with $\mathrm{R}=0.92$. All quantitative MRI parameters are highly significant ( $\mathrm{p}<0.001$ for all). Strongest correlation is seen between T2 and MTR at both thigh and calf level. Constant and slope are similar at thigh and calf level for equivalent correlations. FF: fat fraction; MTR: magnetisation transfer ratio; R : model fit parameter.

Table e5: Linear regression T2 and MTR in muscles fat fraction in the healthy control range (FF $<4 \cdot 8 \%$ thigh; FF $<4 \cdot 7 \%$ calf) in IBM (A) and CMT1A (B) patients and matched controls

| A | Thigh |  |  | Calf |  |  |
| :--- | :---: | :---: | :---: | :---: | :---: | :---: |
| T2 | $\mathrm{R}=0.62, \mathrm{p}<0.0001$ |  |  | $\mathrm{R}=0.52, \mathrm{p}<0.0001$ |  |  |
|  | Co-eff | Std Error | p | Co-eff | Std Error | p |
| Constant | 38.4 | 0.43 | $<0.0001$ | 38.0 | 0.53 | $<0.0001$ |
| IBM | 4.0 | 0.54 | $<0.0001$ | 3.5 | 0.57 | $<0.0001$ |
| FF | 2.52 | 0.21 | $<0.0001$ | 1.78 | 0.25 | $<0.0001$ |
| MTR | $\mathrm{R}=0.61, \mathrm{p}=<0.0001$ |  |  | $\mathrm{R}=0.39, \mathrm{p}<0.0001$ |  |  |
|  | Co-eff | Std Error | p | Co-eff | Std Error | p |
| Constant | 32.9 | 0.16 | $<0.0001$ | 32.3 | 0.20 | $<0.0001$ |
| IBM | -1.5 | 0.19 | $<0.0001$ | -1.1 | 0.21 | $<0.0001$ |
| FF | -0.74 | 0.07 | $<0.0001$ | -0.33 | 0.09 | 0.0007 |


| B | Thigh |  |  | Calf |  |  |
| :--- | :---: | :---: | :---: | :---: | :---: | :---: |
| T2 | $\mathrm{R}=0.49, \mathrm{p}<0.0001$ |  |  | $\mathrm{R}=0.59, \mathrm{p}<0.0001$ |  |  |
|  | Co-eff | Std Error | $p$ | Co-eff | Std Error | $p$ |
| Constant | 38.4 | 0.29 | $<0.0001$ | 36.6 | 0.31 | $<0.0001$ |
| CMT1A | 1.0 | 0.31 | 0.0008 | 2.0 | 0.33 | $<0.0001$ |
| FF | 2.07 | 0.15 | $<0.0001$ | 1.87 | 0.17 | $<0.0001$ |
| MTR | $\mathrm{R}=0.40, \mathrm{p}<0.0001$ |  |  | $\mathrm{R}=0.38, \mathrm{p}<0.0001$ |  |  |
|  | Co-eff | Std Error | $p$ | Co-eff | Std Error | $p$ |
| Constant | 33.0 | 0.12 | $<0.0001$ | 32.8 | 0.14 | $<0.0001$ |
| CMT1A | -0.3 | 0.13 | 0.04 | -0.7 | 0.15 | $<0.0001$ |
| FF | -0.65 | 0.06 | $<0.0001$ | -0.40 | 0.08 | $<0.0001$ |

Determinants of T2 and MTR in muscles with normal FF. FF remains strongly correlated to both T2 and MTR, however subject group (patient $=1$, control $=0$ ) also has a significant effect. R: Overall model correlation coefficient; CMT1A: Charcot-MarieTooth disease type 1A; IBM: inclusion body myositis; FF: fat fraction; MTR: magnetisation transfer ratio; Co-eff: partial regression coefficient; $p$ : significance level.



| †00\％ | E96\％ | $800 \%$ | $000 \% 0$ | 100.0 | $000 \% 0$ | 200\％ | LI0\％ | 250\％0 | d |  |
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| ［0．1，403 |  |  | LWO |  |  | NGI |  |  |  |  |



Table e7: Comparison of outcome measure responsiveness with previous studies in CMT1A

| Measure | Baseline | Change | p | SRM |
| :---: | :---: | :---: | :---: | :---: |
| This study, 1 year |  |  |  |  |
| Mean calf fat fraction (\%) | $15 \cdot 5 \pm 24 \cdot 0$ | $1.22 \pm 1.47$ | $0 \cdot 002$ | 0.83 |
| CMTES (0-28) | $8 \cdot 0 \pm 5 \cdot 1$ | $0 \cdot 3 \pm 1 \cdot 3$ | ns | 0.23 |
| MRC lower limb | $95 \cdot 4 \pm 15 \cdot 4$ | $-0 \cdot 4 \pm 3 \cdot 8$ | ns | -0.11 |
| SF-36 PF (0-100\%) | $65 \cdot 3 \pm 23 \cdot 2$ | $-1.9 \pm 14.9$ | ns | -0.12 |
| Verhamme ${ }^{4}, 5$ years, 46 patients |  |  |  |  |
| Adapted CMTNS^ (0-33) | $11.6 \pm 4.5$ | $1 \cdot 5 \pm 3 \cdot 0$ | 0.003 | 0.49 |
| Nine-hole peg test (s) | $26 \cdot 0 \pm 18 \cdot 4$ | $2 \cdot 0 \pm 5 \cdot 8$ | 0.02 | 0.35 |
| Three-point grip (N) | $7 \pm 32$ | $-6 \cdot 3 \pm 10 \cdot 5$ | <0.001 ${ }^{\text {\# }}$ | -0.60 |
| Ankle dorsiflexion (N) | $190 \pm 74$ | $0 \cdot 1 \pm 28 \cdot 1$ | ns | $0 \cdot 00$ |
| Ankle plantarflexion (N) | $>250{ }^{+}$ | NA | NA | NA |
| Ulnar CMAP (mV) | $4 \cdot 1 \pm 1 \cdot 5$ | $-0 \cdot 4 \pm-0 \cdot 7$ | 0.001* | -0.60 |
| Pareyson ${ }^{6}$, 2 years, 133 patients (placebo arm) |  |  |  |  |
| CMTNS (0-36) | $13 \cdot 9 \pm 4 \cdot 3$ | $0 \cdot 5 \pm 2 \cdot 7$ | <0.05 | $0 \cdot 19$ |
| CMTES (0-28) | $8 \cdot 6 \pm 3 \cdot 6$ | $0 \cdot 5 \pm 2 \cdot 1$ | <0.05 | 0.23 |
| CMT NCS (0-8) | $5 \cdot 2 \pm 1 \cdot 6$ | $-0 \cdot 1 \pm 1 \cdot 6$ | ns | -0.06 |
| Nine-hole peg test (s) | $23 \cdot 4 \pm 5 \cdot 7$ | $0 \cdot 85 \pm 2 \cdot 7$ | <0.01 | 0.31 |
| SF-36 PF (0-100\%) | $62 \cdot 9 \pm 25 \cdot 7$ | $-1 \cdot 1 \pm 15 \cdot 4$ | ns | -0.07 |
| Hand grip (N) | $85 \cdot 8 \pm 38 \cdot 8$ | $-6 \cdot 9 \pm 20 \cdot 3$ | <0.001 | -0.34 |
| Three point pinch (N) | $65 \cdot 2 \pm 29 \cdot 4$ | $-3 \cdot 6 \pm 18 \cdot 8$ | <0.05 | -0.19 |
| Ankle dorsiflexion (N) | $62 \cdot 8 \pm 43 \cdot 1$ | $-9.8 \pm 23 \cdot 7$ | <0.001 | -0.42 |
| Ankle plantarflexion (N) | $97 \cdot 0 \pm 59.7$ | $-2 \cdot 7 \pm 47 \cdot 7$ | ns | -0.06 |
| CMAP sum (mV) | $7 \cdot 1 \pm 4 \cdot 1$ | $0 \cdot 2 \pm 2 \cdot 9$ | ns | 0.08 |

Values expressed mean $\pm$ standard deviation. Non-significant (versus baseline or control) SRM depicted in grey. . \#: identical difference seen in controls; *: greater reduction seen in controls ( $\mathrm{p}=0.05$ ); ${ }^{+}$: measurement limited to 250N; ^: data for this measurement collected retrospectively; NA: not available; ns: not significant; SRM: standardised response mean, calculated from published data as mean change/standard deviation change. Standard deviation in Pareyson study calculated from published $95 \%$ confidence interval by standard statistical formulae: $95 \% \mathrm{Cl}=$ mean -1.96 s.d. to mean +1.96 s.d.; standard error mean $=$ s.d. $/ \mathrm{Vn}$

Figure e1: Correlation of fat fraction with disease duration in IBM and CMT1A patients


Scatter plot of disease duration versus thigh-level (ㅁ) and calf-level (x) fat fraction in IBM and CMT1A patients. In IBM patients positive correlation between disease duration and mean fat fraction is seen at thigh level (rho $=0.50, \mathrm{p}=0.03$ ) but not calf level ( $\mathrm{rho}=0.27, \mathrm{p}=0.28$ ). In CMT1A patients, strong positive correlations at both levels are seen (thigh: rho $=0.81, \mathrm{p}<0.0001$; calf: rho $=0.89, \mathrm{p}<0.0001$ ). The relationship between disease duration and fat fraction appears non-linear in the CMT1A group.

Figure e2: Correlation of MRI measured remaining muscle area with isometric muscle strength


MRI measured RMA of lower limb muscle groups show strong correlation with corresponding strength in IBM (x), CMT1A (+) and controls (o).
A: Right quadriceps. IBM: rho $=0.81, \mathrm{p}<0.0001 ;$ CMT: rho $=0.79, \mathrm{p}<0.0001$; controls: $\mathrm{rho}=0.91, \mathrm{p}<0.0001$
B: Right hamstrings. IBM : $\mathrm{rho}=0.80, \mathrm{p}<0.0001$; CMT: $\mathrm{rho}=0.54, \mathrm{p}=0.02$; controls: $\boldsymbol{r h o}=0.67, \mathrm{p}<0001$
C: Right anterior compartment. IBM: rho $=0.83, \mathrm{p}<0.0001$; CMT: $r$ ho $=0.78, \mathrm{p}<0.0001$; controls: rho $=0.62, \mathrm{p}=0.0007$
D: Right triceps surae. IBM: rho $=0.77, \mathrm{p}<0.0001 ; \mathrm{CMT}$ : rho $=0.72, \mathrm{p}<0.0001$; controls: rho $=0.61, \mathrm{p}=0.0009$

Figure e3: Correlation of calf fat fraction with severity score (CMTES) in CMT1A patients


There is significant correlation between calf muscle fat fraction and CMTES in CMT1A patients (rho=0.63, $\mathrm{p}=0.003$ ). The relationship appears non-linear.

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